

**TITLE**

The variation in pressures exerted by commercially available compression garments

**AUTHOR**

Hill, Jessica; Howatson, Glyn; Van Someren, Ken A.; et al.

**JOURNAL**

Sports Engineering

**DATE DEPOSITED**

7 June 2016

**This version available at**

<https://research.stmarys.ac.uk/id/eprint/1088/>

---

**COPYRIGHT AND REUSE**

Open Research Archive makes this work available, in accordance with publisher policies, for research purposes.

**VERSIONS**

The version presented here may differ from the published version. For citation purposes, please consult the published version for pagination, volume/issue and date of publication.



St Mary's  
University  
Twickenham  
London

OpenResearch  
Archive

## The variation in pressures exerted by commercially available compression garments

*Jessica A. Hill, Glyn Howatson, Ken A. van Someren, Stuart Davidson & Charles R. Pedlar. (2015). The variation in pressures exerted by commercially available compression garments. Sports Engineering.*

Version: Author-accepted manuscript

Copyright and Moral Rights for the articles on this site are retained by the individual authors and/or other copyright owners. For more information on OpenResearch Archive's data policy on reuse of materials please consult <http://research.stmarys.ac.uk/policies.html>

<http://research.stmarys.ac.uk/>

**The variation in pressures exerted by commercially available compression garments**

Original Investigation

1  
2  
3  
4  
5  
6  
7  
8  
9  
10  
11  
12  
13  
14  
15  
16  
17  
18  
19  
20  
21  
22  
23  
24  
25  
26  
27  
28  
29  
30  
31  
32  
33  
34  
35  
36  
37  
38  
39  
40  
41  
42  
43  
44  
45  
46  
47  
48  
49  
50  
51  
52  
53  
54  
55  
56  
57  
58  
59  
60

61 **Abstract**

62 Commercially available compression garments (CGs) demonstrate the enhanced recovery from exercise in  
63 some, but not all studies. It is possible that in some cases the degree of compression pressure (ComP) exerted is  
64 not sufficient to produce any physiological benefit. The aim of this investigation was to identify the levels of  
65 ComP exerted by commercially available CGs. This study was composed of two parts. In part A 50 healthy,  
66 physically active individuals (n=26 male, n=24 female) were fitted with CGs according to manufacturer's  
67 guidelines. ComP was measured in participants standing in the anatomical position with a pressure measurement  
68 device inserted between the skin and the garment. Data were compared to 'ideal' pressure values proposed in  
69 the literature. In part B ComP in three different brands of CG were compared in a population of 29 men who all  
70 wore a medium sized garment. A one way ANOVA indicated that there was a significant difference ( $P<0.05$ )  
71 between observed pressure and ideal pressure at the quadriceps for males and females and in the calf for the  
72 female population. There was no significant difference ( $P>0.05$ ) between observed and ideal pressures in the  
73 calf of the male population. No significant differences in pressure ( $P>0.05$ ) were observed between CG brands  
74 at the quadriceps or calf. In conclusion a large number of individuals may not be experiencing an adequate  
75 ComP from CG, and this is true for all 3 of the major brands of CGs tested in this investigation.

76  
77 Keywords: Recovery, Stockings, Tights, Sports, Athletes

78  
79  
80 **Introduction**

81 The use of commercially available compression garments (CGs) is becoming increasingly popular within an  
82 athletic setting [1-3]. It is claimed that CGs can improve performance, reduce fatigue and enhance recovery  
83 [4]. However, the known studies show mixed results, with some supporting the use of CGs [5-8] and others  
84 observing no benefits [9]. Compression pressure (ComP) seems to be one of the major factors that potentially  
85 determines their efficacy.

86  
87 Manufacturers recommend that lower limb CGs (tights) are fitted according to the height and mass of an  
88 individual [10], however, the variation in limb size and tissue structure within a given population is likely to  
89 affect the fit, particularly when standard sizing categories are used [11]. Thus wide inter-individual variation  
90 may exist in the ComP exerted by CGs [12]. Ashdown [13] also indicated that sizing systems used to create  
91 'ready to wear' garments are flawed, due to the lack of size variation available to fit the wide range of body  
92 types within a population. A large number of studies do not specifically measure the ComP exerted by the CGs  
93 used within their study. These studies either fail to report the level of ComP altogether [8, 14-16], report the  
94 ComP indicated by the manufacturers of the product, or reference ComP reported in previous research that has  
95 used the same brand of garment [11, 17-20]. It has been suggested that the measurement of interface pressure  
96 between the skin and the garment is essential in evaluating the efficacy of a garment [21]. Consequently, the  
97 ComP should be measured for each individual because the degree of compression exerted by a garment is  
98 dependent on the individual size and shape of the body [20] and not necessarily on the height and mass.

99  
100 To date, the ideal ComP required to be beneficial to performance and recovery has not been defined. CGs,  
101 particularly lower limb garments, are purported to be graduated, with the highest ComP exerted at the ankle and  
102 decreasing towards the thigh, thereby creating a pressure gradient [22]. Reported (but not specifically verified)  
103 levels of ComP exerted by CGs used in recent research range from 10-12 mmHg [19] to 18-22 mmHg [11].  
104 Clinical grade CGs exerting pressures of 30-60 mmHg are frequently prescribed for a range of medical purposes  
105 [23]. It has been suggested that for compression to be effective in modulating haemodynamic factors, the ComP  
106 must be sufficient to cause a narrowing of the superficial blood vessels; and in order for this to occur the  
107 compression must be greater than intravenous pressure [24]. In a supine position, venous pressure in the lower  
108 limb is approximately 10-15 mmHg, however these pressures are much higher when standing (30-90 mmHg)  
109 [24]. This indicates that the level of compression required to be of benefit may be dependent upon body  
110 position. Compression pressures of 10-15 mmHg have been shown to be effective in reducing the diameter of  
111 superficial veins in a supine position, however much higher pressures are required to achieve the same results  
112 when standing [24]. In contrast, Watanuki and Murata [25] observed improved cardiac output and venous  
113 return with ComP of 20 mmHg at the thigh and 25 mmHg at the calf. The authors of this study estimated that  
114 the minimum ComP required to improve venous return is 17.3 mmHg at the calf, decreasing to 15.1 mmHg at  
115 the quadriceps. Hypothetically, if individuals are not receiving a physiologically effective ComP, the CGs may  
116 have no effect on recovery or performance.

117  
118  
119  
120

121 Ali et al [26] investigated the effects of different grades of compression garments with high (32mmHg at the  
122 ankle and 23mmHg at the knee) low (15mmHg at the ankle and 12mmHg at the knee) and no compression, on  
123 40 minute running performance. Although no benefits of the compression garments were observed on  
124 performance or recovery, participants found the low grade compression garments more comfortable. Whilst  
125 there are no studies that indicate optimal levels of compression in the sporting field, clinical research had found  
126 positive results with ComP of 15-30 mmHg at the ankle dissipating at the thigh [26-28]. Research has also  
127 indicated that high ComP (approximately 30 mmHg at the calf) may impair blood flow and restrict venous  
128 return [29]. With this in mind the ComP observed in this study is compared to the ComP suggested by  
129 Watanuki and Murata [25].

130  
131  
132 Current evidence for the benefits of using CGs remains equivocal or weak at best. This may be because the  
133 popular commercially available garments do not exert sufficient enough pressure to be of benefit. Defining the  
134 exact ComP achieved with CGs would enable detailed investigations into the optimum ComP required to affect  
135 performance and recovery, and will improve our ability to interpret research findings [12]. Therefore the  
136 primary aim of this investigation was to identify the ComP exerted by commercially available lower limb CGs  
137 across a representative sample of physically active male and female population. The secondary aim was to  
138 identify whether there was consistency in the amount of ComP exerted between different brands of similar  
139 products.

## 141 **Methodology**

### 142 **Participants**

143 This study was composed of two parts.

144  
145  
146 Fifty participants, having different body sizes (male: n=26; female: n=24), were recruited to participate in part A  
147 of the study, in order to establish ComP exerted by commercially available garments. Twenty nine male  
148 participants were recruited to participate in Part B of the study, in order to investigate variability in ComP for  
149 different product brands. A medium sized garment from 3 different brands was selected (participant  
150 characteristics can be seen in table 1). All participants were healthy, physically active and exercised minimum 3  
151 times per week. Procedures were approved by the University ethics committee, in accordance with the  
152 Declaration of Helsinki and all participants gave written, informed consent and completed a health screening  
153 questionnaire. Participants were asked to refrain from heavy exercise in the 48 h preceding the testing session  
154 and were excluded from the study if they had a chronic illness or if they were experiencing any musculoskeletal  
155 pain or discomfort.

### 156 **Procedures**

157  
158 Anthropometric data were collected from all participants including height and weight; waist, hip and gluteal  
159 circumference; thigh, calf and ankle girth and skinfold measurements from 7 sites (bicep, tricep, subscapular,  
160 supraspinale, abdomen, front thigh and medial calf). All girth and skinfold measures were taken from the right  
161 leg, in accordance with ISAK guidelines. All measures were taken by a level 2 anthropometrist. The technical  
162 error of measurement (TEM) for each anthropometric variable is reported in Table 2.

163  
164  
165 Following anthropometric data collection, male and female participants in part A of the study were fitted with a  
166 pair of CGs from one brand (2XU, MA1551b men's compression tights or WA1552b women's compression  
167 tights, Melbourne, Australia). Garments were fitted based upon the height and weight of the participant,  
168 according to manufacturer guidelines. All participants were either a small, medium or large in traditional  
169 garment size (none of the participants required a tall sized garment).

170  
171 Part B involved a comparison between 3 different brands of CGs in male participants only. Garment A (2XU,  
172 MA1551b men's compression tights) fitted participants in a height and weight range of 150-185cm and 65-90kg  
173 respectively, garment B (Skins, A400 men's compression tights, Campbelltown, Australia) fitted participants in  
174 a height and weight range of 170-190cm and 70-85kg respectively and garment C (Linebreak, men's velocity  
175 compression tights, Sydney, Australia) fitted participants in a height and weight range of 157-190cm and 65-  
176 75kg respectively. Garments A, B and C were fitted, in a randomised order, to all male participants who met the  
177 manufacturer's fitting criteria (the characteristics for each group can be seen in Table 3). Garments A, B and C  
178 were selected for use in this study as they were the most frequently used garments for known research studies  
179 investigating the efficacy of lower limb compression tights on sport performance and recovery [5,10-11,15-16].

180 Of the 20 studies, garment A was used in 3 studies, garment B was used in 11 studies and garment C was used  
181 in 4 studies.

182 The ComP was measured using a pressure measuring device (Kikuhime, TT Medi Trade, Søleddet, Denmark)  
183 that has previously been validated for use with compression clothing [12]. The device was calibrated at the  
184 National Physical Laboratory using a pressure vessel (OerLikon Leybold Vacuum, GmbH, Cologne, Germany)  
185 attached to a digital pressure controller (DPI 500, Digital Pressure Controller, Druck Ltd, Leicester). The ComP  
186 was measured at 3 sites: the midpoint between the inguinal crease and the superior aspect of the patella of the  
187 front thigh; the medial aspect of the calf at the site of maximal girth; and 2 cm above the centre of the medial  
188 malleolus of the ankle. The seam on the ankle of the garment was positioned below the distal border of the  
189 malleolus. All measurements taken with the pressure measuring device were clear of the seam on the lower  
190 edge of the garment and clear of the vertical seam on the garment. ComP measurements were taken with the  
191 participant standing in the anatomical zero position with their weight evenly distributed on both feet.  
192 Measurements were repeated 3 times with the mean value recorded. Technical error of measurement (TEM) was  
193 0.48 and 0.92 mmHg at the quadriceps and calf, respectively. The pressure measuring device displays values to  
194 the nearest 1 mmHg.

195

### 196 **Data Analysis**

197 Data collected in part A were analysed using one-way analysis of variance (ANOVA). In the absence of a  
198 defined optimal ComP, compression at the quadriceps and calf for a male and female population compared to  
199 the minimum recommended ComP of 17.3 and 15.1 mmHg as suggested by Watanuki and Murata, (1994). Data  
200 collected in part B were analysed using a one-way ANOVA. A Pearson correlation was also carried out to  
201 identify whether any of the measured anthropometric characteristics were related to the ComP at the quadriceps  
202 and calf. Where significant differences were observed a *post-hoc* test with a Fisher least significant difference  
203 (LSD) adjustment was used to highlight where the differences occurred. Data is presented as a mean value and  
204 standard deviations. Significance was set at  $p \leq 0.05$ .

205

### 206 **Results**

207 The anthropometric characteristics of the participants are reported in tables 1 and 3. A one-dimensional  
208 ANOVA indicated that there was a significant group difference ( $F_{2,77}=92.644$ ,  $p < 0.001$ ) for ComP achieved at  
209 the quadriceps. Further *post-hoc* analysis indicated that ComP in the male population was significantly lower  
210 ( $p < 0.001$ ) than the recommended minimum pressure. ComP at the quadriceps was  $9.9 \pm 2.9$  mmHg, failing to  
211 meet the minimum recommended ComP of 15.1 mmHg by 34.4% (Figure 1). ComP achieved in the female  
212 population was also significantly lower than the recommended ComP ( $p < 0.001$ ). The average ComP of  $7.9 \pm 1.7$   
213 mmHg fell short of the recommended ComP by 47% (Figure 1).

214

215 A significant group difference was also observed for ComP achieved at the calf ( $F_{2,77}=11.535$ ,  $p < 0.001$ ). Post  
216 hoc analysis indicated that there was no significant difference ( $P=0.605$ ) between ideal ComP and ComP at the  
217 calf in the male population. Pressure fell short of the recommended level of 17.3 mmHg by 2.9%. There was  
218 however, a significant difference between ideal ComP and ComP at the calf in the female population ( $p < 0.001$ ).  
219 The mean ComP observed at the female calf was  $13.9 \pm 2.3$  mmHg failing to meet the suggested minimum ComP  
220 by 19.7% (Figure 1). Individual compression values for the quadriceps and calf can be seen in figure 2.

221

222 The second part of the investigation revealed no significant difference in ComP between garment brands at the  
223 quadriceps ( $p=0.638$ ) and the calf ( $p=0.318$ ). Compression at the quadriceps fell short of the ideal minimum  
224 pressure by 33.2, 28.9 and 30.5% for brands A, B and C respectively; ComP at the calf did not achieve the ideal  
225 minimum pressure by 10.5, 13.5 and 4.2% for brands A, B and C respectively (Figure 3). There were no  
226 significant correlations ( $p > 0.05$ ) between any anthropometric variable measured and ComP at the quadriceps  
227 and calf.

228

229

### 230 **Discussion**

231 The primary aims of this investigation were to 1) ascertain the level of ComP exerted by a commercially  
232 available CGs when applied to the lower limb in a population of active participants; and 2) to identify whether  
233 there was consistency in ComP between different popular brands. Results indicated that there was a large  
234 degree of variability in ComP when garments were fitted according to manufacturer's guidelines. In part A,  
235 ComP ranged from 4-16.7 mmHg at the quadriceps and from 10.3-25 mmHg at the calf. In part B ComP ranged  
236 from 8-15 and 10.3-15 mmHg for garment A, 7.7-16 and 9-22 mmHg for garment B and 6-15 and 10.7-22  
237 mmHg for garment C at the quadriceps and calf respectively.

238  
239  
240  
241  
242  
243  
244  
245  
246  
247  
248  
249  
250  
251  
252  
253  
254  
255  
256  
257  
258  
259  
260  
261  
262  
263  
264  
265  
266  
267  
268  
269  
270  
271  
272  
273  
274  
275  
276  
277  
278  
279  
280  
281  
282  
283  
284  
285  
286  
287  
288  
289  
290  
291  
292  
293  
294  
295  
296  
297

In addition, ComP fell short of the minimum pressure, suggested by Watanuki and Murata [25], in both the male and female populations at the quadriceps. ComP also fell short of the minimum pressure in the female population at the calf. When three different brands of CG were compared there were no significant differences in ComP at the quadriceps or the calf. It should also be noted that a medium sized CG in three different brands does not fit the same sized population. Garment A was the smallest fitting a height and weight range of 157-190cm and 65-75kg, followed by garment B fitting a height and weight range of 170-190cm and 70-85kg, and C was the largest fitting a height and weight range of 150-185cm and 65-90kg. The difference in populations can be observed in Table 3.

Previous research has caused concerns over whether standardised size categories are effective due to the large variations in anthropometric characteristics within a given population [11]. MacRae et al. [30] indicated that people categorised into one garment size classification, will vary in body shape and size. Indeed this is true of the participants who took part in this study. For example, those fitted with garment brand A exhibited a thigh and calf circumference that ranged from 46.1-56.3 and 33.0-39.5 cm respectively, despite them all meeting the manufacturers recommendations for fitting a medium size garment. It should be acknowledged that some manufacturers now offer bespoke garments, fitted with greater precision by using more surface measurements or using a body scanning device. It is likely that these approaches will improve garment fit and possibly increase the level and consistency of ComP.

The findings of this investigation support concerns identifying that there is wide variation in body morphology and ComP exerted by the CGs tested here. ComP ranged from 4-16.7 mmHg at the quadriceps and 10.3-25 mmHg at the calf in the male population and 5-12.7 mmHg at the quadriceps and 10.3-18.7 mmHg at the calf in the female population. This observation indicates that the suggested minimum pressures of 15.1 mmHg at the quadriceps and 17.3 mmHg at the calf were not being met for the majority of individuals. Individual ComP observed in figure 2 demonstrate the large range in pressure received amongst participants at the quadriceps and calf. Individual data was used for the correlational analysis, the fact that there were no correlation between any anthropometric variable and quadriceps or calf ComP indicates there is a more complex interaction between various anthropometric characteristics and ComP applied by the CGs. This is supported by Troynikov et al [4], who highlighted the need for further investigation into the interaction between the CG and the body of the individual using the garment.

There is no current consensus on how much ComP is required in order to improve indices of performance and recovery. Many of the observed improvements in haemodynamics and subsequent recommendations on the application of compression are derived from clinical studies [28,31]. Brandages et al [31] used CGs that exerted a ComP of 40 mmHg at the ankle decreasing to 21 mmHg at the calf and Ibegbuna et al. [28] used CGs with a reported range of 18-24 mmHg. These ComP appear to have crossed over into the sporting arena with little evidence to suggest the ComP levels are optimum or even effective. It may therefore be possible that the levels of ComP used to treat clinical conditions may not be necessary in an athletic setting [2,32]. Ali et al [2] investigated the effects of three different grades of below the knee, lower limb CGs, low (12-15 mmHg), medium (18-21 mmHg) and high (23-32 mmHg). This study observed that jump height was improved, following a bout of endurance exercise, when participants wore the low and medium grade garments, but not the high grade garment. The authors suggest that muscle function was better maintained in the low and medium grade trials but more research is needed to understand why no improvement was observed in the high grade trial. These findings highlight the importance of understanding factors affecting CG fit, particularly in a performance setting.

### Conclusion

A large number of individuals are using CGs to enhance performance or recovery [6], however this investigation demonstrates that the majority of people who use these garments may not be receiving adequate levels of ComP to be of benefit. In addition to this there is a large variation in the range of ComP received from the same brand of garment across a population. This has implications for individuals who wish to use CGs and indicates the need to measure the exact amount of ComP exerted by a CG on each individual.

Knowledge on the ComP individuals receive from these garments is key to interpreting the findings from studies investigating the efficacy of CGs [12], and a greater level of rigour is needed in order to define the ComP achieved in studies of compression garments in sports applications. Given the large range in ComP observed in this study, it is possible that whilst some individuals are receiving insufficient ComP to be of benefit, perhaps others are receiving excessive ComP. This highlights the need to measure ComP pressure in all individuals and

298 may explain why literature investigating the efficacy of CGs is inconsistent, particularly as the majority of the  
299 research failed to report the ComP applied to the limb. Future research should 1) measure and control for the  
300 pressures exerted by commercially available CGs; 2) investigate whether bespoke fitted garments improve  
301 ComP and consequently recovery; 3) identify the effects of different levels of ComP on indices of performance  
302 and recovery.  
303

### 304 **Conflict of Interest**

305 The authors declare they have no conflict of interest.  
306  
307

### 308 **References**

- 309 1. Troynikov O, Wardiningshi W, Koptug A, Watson C (2013) Influence of material properties and garment  
310 composition on pressure generated by sport compression garments. *Procedia Eng* 60:157-162  
311
- 312 2. Ali A, Creasy RH, Edge JA (2011) The effect of graduated compression stockings on running performance. *J*  
313 *Strength Cond Res* 25:1385-1392  
314
- 315 3. Doan BK, Kwon Y, Newton RU, Shim J, Popper EM, Rogers RA, Bolt LR, Robertson M, Kraemer WJ  
316 (2003) Evaluation of a lower body compression garment. *J Sport Sci* 21:602-610  
317
- 318 4. Troynikov O, Ashayeri E, Burton M, Subic A, Alam F, Marteau S (2010) Factors influencing the  
319 effectiveness of compression garments used in sports. *Procedia Eng* 2:2823-2829  
320
- 321 5. Hill J, Howatson G, van Someren K, Walshe I, Pedlar C (2014) The influence of compression garments on  
322 recovery following Marathon running. *J Strength Cond Res*  
323
- 324 6. Hill J, Howatson G, van Someren K, Leeder J, Pedlar C (2013) Compression garments and recovery from  
325 exercise-induced muscle damage. A Meta-Analysis. *Brit J Sport Med* doi:10.1136/bjsports-2013-092456  
326
- 327 7. Bottaro M, Martorelli S, Vilaça J (2011) Neuromuscular compression garments: Effects on neuromuscular  
328 strength and recovery. *JHK* 1:27-31
  
- 329 8. Kraemer WJ, Flanagan SD, Comstock BA, Fragala MS, Earp JE, Dunn-Lewis C, Ho J, Thomas GA,  
330 Solomon-Hill G, Penwell ZR, Powell MD, Wolf MR, Volek JS, Denegar CR, Maresh, CM (2010) Effects of a  
331 whole body compression garment on markers of recovery after a heavy resistance workout in men and women.  
332 *J Strength Cond Res* 24:804-814  
333
- 334 9. Carling J, Francis K, Lorish C (1995) The effects of continuous external compression on delayed-onset  
335 muscle soreness (DOMS). *Int Journal Rehabil Health* 1:223-235  
336
- 337 10. Scanlan AT, Dascombe BJ, Reaburn PR, Osborne M (2008) The effects of wearing lower-body compression  
338 garments during endurance cycling. *Int J Sports Physiol Perform* 3:1137-1144  
339
- 340 11. Davies V, Thompson KG, Cooper SM (2009) The effects of compression garments on recovery. *J Strength*  
341 *Cond Res* 2:1786-1794  
342
- 343 12. Brophy-Williams N, Driller MW, Halson SL, Fell JW, Shing CM (2013) Evaluating the Kikuhime pressure  
344 monitor for use with sports compression clothing. *Sp Eng* 1-6  
345
- 346 13. Ashdown SP (1998) An investigation of the structure of sizing systems. A comparison of three  
347 multidimensional optimised sizing systems generated from anthropometric data with the ASTM standard D558-  
348 94. *Int J Cloth Sci Tech* 10:324-341  
349
- 350 14. Bringard A, Perrey S, Belluye N (2006) Aerobic energy cost and sensation responses during submaximal  
351 running exercise – positive effects of wearing compression tights. *Int J Sports Med* 27:373-378  
352
- 353 15. Gill ND, Beaven CM, Cook C (2006) Effectiveness of post-match recovery strategies in rugby players. *Brit*  
354 *J Sport Med* 40:260-263  
355



- 356 16. Higgins T, Naughton GA, Burgess D (2009) Effects of wearing compression garments on physiological and  
357 performance measures in a simulated game-specific circuit for netball. *J Sci Med Sport* 12:223-226  
358
- 359 17. Ali A, Caine MP, Snow BG (2007) Graduated compression stockings: Physiological and perceptual  
360 responses during and after exercise. *J Sports Sci* 25:413-419  
361
- 362 18. Chatard JC, Atlaoui D, Farjanel J, Louisy F, Rastel D, Guezennec CY (2004) Elastic stockings, performance  
363 and leg pain recovery in 63-year-old sportsmen. *Eur J Appl Physiol* 93:347-352  
364
- 365 19. French DN, Thompson KG, Garland SW, Barnes CA, Portas MD, Hood PE, Wilkes G (2008) The effects of  
366 contrast bathing and compression therapy of muscular performance. *Med Sci Sports Exerc* 40:1297-1306  
367
- 368 20. Jakeman JR, Byrne C, Eston RG (2010) Lower limb compression garment improves recovery from exercise  
369 induced damage in young, active females. *Eur J Appl Physiol*. 109:1137-1144  
370
- 371 21. Partsch H, Clark M, Bassez S, Benigni JP, Becker F, Blazek V, Caprini J, Cornu-Thenard A, Hafner J, Flour  
372 M, Jugner M, Morratt C, Newmann M (2006) Measurement of lower leg compression in vivo: recommendations  
373 for the performance of measurements of interface pressure and stiffness. *Dermatol Surg* 32:224-233  
374
- 375 22. Bryne B (2001) Deep vein thrombosis prophylaxis: The effectiveness and implications of using below-knee  
376 or thigh-length graduated compression stockings. *Heart Lung* 30:277-284  
377
- 378 23. Brennan MJ, Miller LT (1998) Overview and treatment options and review of the current role and use of  
379 compression garments, intermittent pumps, and exercise in the management of lymphedema. *Cancer* 83:2821-  
380 2827  
381
- 382 24. Partsch H, Mosti G (2008) Thigh compression. *Phlebology* 23:252-258  
383
- 384 25. Watanuki S, Murata H (1994) Effects of wearing compression stockings on cardiovascular responses. *Ann*  
385 *Physiol Anthropol* 13:121-121  
386
- 387 26. Ali A., Creasy RH. and Edge JA (2010) Physiological effects of wearing graduated compression stockings  
388 during running. *Eur J Appl Physiol* 109:1017-1025  
389
- 390 27. Agu O, Baker D, Seifalian AM (2004) Effect of graduated compression stockings on limb oxygenation and  
391 venous function during exercise in patients with venous insufficiency. *Vascular* 12:69-76  
392
- 393 28. Ibegbuna V, Delis KT, Nicolaidis AN, Aina O (2003) Effect of elastic compression stockings on venous  
394 hemodynamics during walking. *J Vasc Surg* 37:420-425  
395
- 396 29. Lawrence D, Kakkar VV (1980) Graduated, static, external compression of the lower limb: A physiological  
397 assessment. *Br J Surg* 67: 119-121.  
398
- 399 30. MacRae BA, Cotter JD, Laing RM (2011) Compression garments and exercise: garment considerations,  
400 physiology and performance. *Sports Med* 41:815-43  
401
- 402 31. Brandjes DP, Büller HR, Heijboer H, Huisman MV, de Rijk M, Jagt H (1997) Randomised trial of effect of  
403 compression stockings in patients with symptomatic proximal-vein thrombosis. *Lancet* 349:759-762  
404
- 405 32. Dascombe BJ, Hoare TK, Sear JA, Reaburn PR, Scanlan AT (2011) The effects of wearing undersized  
406 lower-body compression garments on endurance running performance. *Int J Sports Physiol Perform* 6:160-173  
407  
408  
409